Abstract: A method to detect NMR spectra from heteronuclei through the modulation that they impose on a water resonance is exemplified. The approach exploits chemical exchange saturation transfers, which can magnify the signal of labile protons through their influence on a water peak. To impose a heteronuclear modulation on water, an HMQC-type sequence was combined with the FLEX approach. 1D $^{15}$N NMR spectra of exchanging sites could thus be detected, with about tenfold amplifications over the $^{14}$N modulations afforded by conventionally detected HMQC NMR spectroscopy. Extensions of this approach enable 2D heteronuclear acquisitions on directly bonded $^{1}$H–$^{15}$N spin pairs, also with significant signal amplification. Despite the interesting limits of detection that these signal enhancements could open in NMR spectroscopy, these gains are constrained by the rates of solvent exchange of the targeted heteronuclear pairs, as well as by spectrometer instabilities affecting the intense water resonances detected in these experiments.

Nuclear magnetic resonance (NMR) is often hampered by its low sensitivity. Several approaches have emerged to overcome this, including hardware improvements[1] and methods for enhancing the signals of liquids and solids by nuclear hyperpolarization.[2] Foremost among the sensitivity-challenged applications of NMR is in vivo spectroscopy, where averaging times are by necessity capped and where hardware options are limited by the physical characteristics of the sample. A breakthrough in in vivo NMR spectroscopy occurred with the advent of chemical exchange saturation transfer (CEST).[3] which exploits the transfer of saturation from labile protons to water to facilitate the detection of the former in metabolites, customized contrast agents, and tissue macromolecules.[4] Instead of using a single transfer to observe the evolution of these labile sites, as in exchange spectroscopy,[5] CEST relies on prolonged, frequency-selective saturation of the labile protons, followed by a transfer of this effect to the much stronger solvent resonance. This forfeits the possibility of achieving a broadband interrogation of the full spectrum; yet this is compensated by the potential amplification of the frequency-selective information by multiple solute–solvent exchanges. Such exchanges will enhance the saturation by factors on the order of $k_{ex}T_{1}^{obs}$, where $k_{ex}$ is the rate of solvent exchange with the labile proton, and $T_{1}^{obs}$ is the relaxation time of the observed water molecules. This product can lead to orders-of-magnitude signal enhancements with respect to a single labile proton response. CEST has thus enabled the 3D NMR imaging of previously unmappable species, including glucose,[6a] urea,[6b] creatine,[7] and intrinsic proteins,[8] and is rapidly becoming a valuable alternative for investigating health, disease, and homeostasis in both animals and humans.[6, 7]

Despite these major sensitivity benefits, efforts still continue to reinstate the speed and multiplexing benefits that are common in Fourier transform (FT) NMR spectroscopy into CEST. These endeavors led to the possibility of collecting broadband spectral information by the application of suitably tuned field gradients[9] and, most relevant for the present work, by the establishment of Fourier-based alternatives for both thermally and hyperpolarized samples.[9–11] In the frequency labeled exchange (FLEX) experiment, for instance, the solute spectral region to be targeted is initially encoded by a pair of selective excitation/storage pulses separated by a delay $t_{1}$ that will modulate the amplitudes of the magnetizations of the labile sites. However, rather than observing these directly after an exchange with the solvent, FLEX loops this process numerous times, magnifying the encoding effects onto the water resonance, and imposing a modulation on the latter that is much larger than what a single mixing would afford. Repeating this as a function of $t_{1}$ and applying a single, final observation pulse on the water molecules after each encoding, enables after 2D FT the spectral detection of the labile protons with an increased sensitivity. Very recently,[12] this effect was extended by the use of an $^{15}$N-selective BIRD pulse,[13] transferring the $^{15}$N presence to bonded urea protons with a 0/180° amplitude modulation. By performing a $^{1}$H-based FLEX experiment on the latter, a water image with a $^{15}$N-encoded saturation effect of up to 25% was obtained. The present study elaborates these ideas in a related but different direction, by introducing an approach that exploits their advantages while seeking a full time-domain encoding of the heteronuclear dimension. To achieve this, the principles underlying FLEX[12] were combined with those of HMOC experiments that avoid the excitation of water.[14] This opens up new possibilities to record 1D $^{15}$N NMR spectra from sites connected to labile protons as well as 2D correlation spectra between the $^{15}$N nuclei and these labile hydrogen atoms. In both cases, these heteronucleus-oriented experiments ended up being observed on water, thereby benefiting from the type of sensitivity enhancement that characterizes CEST.
To explore these ideas further, pulse sequences for what we denominate “heteronuclear FLEX” (HetFLEX) were written (Figure 1a), both in a 1D form encoding solely the $^{15}$N evolution and as a 2D $^{15}$N–$^1$H extension. To incorporate all desired elements, these sequences began with a chemical-shift-specific creation of heteronuclear $H_nN_m$ states, using selective 90° pulses that exclusively address the NH spectral region.$^{[18]}$ These coherences were allowed to evolve under the action of the $^{15}$N chemical shift, and the resulting $\cos(\omega t T_1)$ amplitude modulation was transferred back to the adjacent proton. Then, instead of detecting the ensuing transverse $^1$H coherences as in HMQC, these were stored onto $H_1$ as per the dictates of FLEX, and allowed to undergo exchange with the hitherto untouched magnetization of water over a mixing period $t_{\text{exch}}$. This procedure was repeated $N$ times to enhance the modulation on the water up to a plateau constrained by $T_1$ of the water. Finally, the water signal was detected with full or partial excitation for each $t_1$ encoding increment, delivering the heteronucleus-imposed modulation in its amplitude. Figure S1 in the Supporting Information illustrates how the resulting modulations look like for 1D acquisitions using $t_1$ as the sole $^{15}$N modulation variable, as well as for 2D $^{15}$N/$^1$H spectral correlations employing $t_1/t_2$ increments. Data are also shown for experiments involving a single scan per $t_1$, where the desired modulations ride on top of a pedestal arising from the non-exchanged water molecules, and for two scan experiments where the water pedestal is subtracted by $^{15}$N phase cycling. For both instances, quadrature components can be generated by using orthogonal pulse phases, enabling a sign discrimination of the HetFLEX resonance position.$^{[18]}$ 1D spectra acquired after Fourier transforming signals acquired using this sequence are compared against 1D traces arising from $^1$H-detected HMQC acquisitions performed using identical selective pulses but no water signal manipulations in Figure 1b–e. These data confirm a per-scan increase in the $^{15}$N intensity modulation upon relying on the water detection, ranging from 13 to 30 times that of HMQC. Although these are auspicious enhancements, we see that the noise in HetFLEX is also magnified, depriving the spectra from translating these signal enhancements into equal signal-to-noise ratio (SNR) gains; compared to HMQC-derived 1D $^{15}$N spectra, HetFLEX SNRs are solely enhanced by a factor of 2–5. This HetFLEX noise does not appear to be thermal, but rather originate from “t-noise”$^{[15]}$ associated with the detection of a concentrated water signal in these experiments. Efforts are under way to attenuate these in-principle removable effects, by perfecting the experimental setup and by deconvolution methods. Still, it is interesting to note that comparisons between 1D $^{15}$N NMR traces arising from HetFLEX and HMQC acquisitions yield remarkably similar results, not only for single amine and amide moieties, but also for more complex samples. Figure 1d shows this similarity for a 3 kDa cutoff lysate composed of several peptides that are essentially unstructured, and hence significantly exposed to water. Finally, the water signal was detected with full or partial excitation for each $t_1$ encoding increment, delivering the heteronucleus-imposed modulation in its amplitude.

Figure 1. a) Pulse scheme of the HetFLEX experiment. $t_1$ and $t_2$ are the $^{15}$N and $^1$H encoding delays; open shapes correspond to frequency-selective 90° or 180° pulses; filled black rectangles are hard 90° pulses; $G_1$, $G_2$, and $G_3$ are purging gradients; $\Delta$ corresponds to 1/2$J$, and $\phi$ is a factor compensating for the width of the sinc pulse. Following the second $^{15}$N pulse, a $\Delta-\phi$ delay is used for 1D experiments, whereas for 2D experiments, $t_2$ is added. As a constant $t_{\text{prep}}$ time is used for each loop within brackets, the exchange time varies slightly depending on the $t_1$ and $t_2$ increments; this is done in order to minimize relaxation weightings for different encodings. $\phi$ was incremented by 90° to achieve quadrature detection$^{[18]}$ and phase-cycled as $\pm x$ together with $\phi_2$ to achieve water cancellation. b–e) 1D $^{15}$N spectra extracted from conventional 2D HMQC (left) and HetFLEX data (right) for different $^{15}$N-labeled samples. Both sequences were applied on the same samples using identical pulses and gains, the same number of $t_1$ increments (64), equal numbers of scans per increment (2), identical recycle delays (2 s), and equal pulses (other than for the final 90° $^1$H pulse and purging gradient, omitted in the HMQC). The factors in the HMQC column reflect the vertical scale amplifications used to bring the HMQC traces to the same intensity as their HetFLEX counterparts. All spectra were acquired at 23.5 °C except for that of the lysate, which was collected at 37 °C; see the Supporting Information for further details.
transfer and the solvent magnetization transfer processes. All these, as well as the various $T_1$ values involved, will determine the sensitivity and therefore the practicality of the experiment. To assess the influence of some of these parameters, a sample of alanine in $D_2O/H_2O$ (2:8) at pH 2.2 was examined. Table 1 presents the effect of temperature on the

<table>
<thead>
<tr>
<th>Temperature (°C)</th>
<th>$\Delta_{\text{HMQC}}^\text{FD}/I_{\text{HMQC}}$</th>
<th>$\Delta_{\text{FLEX}}^\text{FD}/I_{\text{FLEX}}$</th>
<th>$\Delta_{\text{HetFLEX}}^\text{FD}/I_{\text{HetFLEX}}$</th>
</tr>
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<tbody>
<tr>
<td>6.5</td>
<td>78 ± 8</td>
<td>3.8 ± 0.7</td>
<td>2.7 ± 0.3</td>
</tr>
<tr>
<td>10.0</td>
<td>70 ± 3</td>
<td>4.3 ± 0.1</td>
<td>3.5 ± 0.1</td>
</tr>
<tr>
<td>17.0</td>
<td>68 ± 0.5</td>
<td>6.4 ± 0.1</td>
<td>4.6 ± 0.1</td>
</tr>
<tr>
<td>23.5</td>
<td>17 ± 3</td>
<td>17.2 ± 0.5</td>
<td>3.1 ± 0.1</td>
</tr>
<tr>
<td>29.5</td>
<td>4.9 ± 0.9</td>
<td>13.1 ± 0.2</td>
<td>0.6 ± 0.1</td>
</tr>
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These data are plotted normalized by both the number of acquisitions and by the unit acquisition time. An exponential increase in intensity occurs as a function of $N$ until $N_{\text{prep}} = T_1^{15N}$; the water $T_1$ thus controls the maximum achievable enhancement, as exemplified by the different plateaus shown in Figure 2b upon increasing the concentration of a relaxation agent. Note that while the absolute HetFLEX enhancements decrease upon reducing the $T_1$ of water, the fact that $N_{\text{prep}}$ governs the repetition time of each scan means that shortening the relaxation of water can actually lead to further SNR advantages versus HMQC when viewing the experiment in terms of the acquisition time (Figure 2c). For the chosen $t_{\text{exch}} = 40$ ms, for instance, setting $N = 64$ yields approximately 90% of the maximum signal obtained within reasonably short acquisition times. In an additional set of experiments, Figure 2d illustrates how different combinations of $t_{\text{exch}}$ and $N$ yielding the same total exchange period of $64 \times 40$ ms = 2.56 s modulate the overall HetFLEX intensity. The behavior is clearly non-monotonic, and confirms the existence of an optimum $t_{\text{exch}}$ value.

As mentioned, the HetFLEX sequence can be modified to include a second increment, $t_2$, to encode the $^1$H evolution of the NH moieties (Figure 1a). This evolution will modulate the hetronuclear one, leading to the storage of an $^1$H magnetization whose overall dependence will be $C_0 \sin(\omega t_1) + C_2 \sin(\omega t_2)$. As this modulation will be conveyed to the water signal intensity by the exchange process, nested $t_1$ and $t_2$ evolutions lead to the possibility of utilizing water to detect 2D-HMQC-like data. Figure 3 exemplifies these solvent-based 2D acquisitions, applied to the amino acids and peptides that were targeted by 1D HetFLEX. Upon

**Table 1:** Amplitudes of the $^{15}$N-driven modulations [%] measured in HMQC, FLEX, and HetFLEX on aqueous alanine at different temperatures.\(^{[56]}\)

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observed HetFLEX modulation, and analyzes it in terms of its two governing processes, namely the HMQC transfer efficiency and the FLEX efficiency. The former steadily degrades with temperature as a result of the increased solvent exchange rate. At the same time, the $^1$H FLEX efficiency improves because of the increase in exchange rate. The overall HetFLEX outcome closely follows the product between the efficiencies observed for these two modules, $\Delta_{\text{HetFLEX}}^\text{FD} = \Delta_{\text{HMQC}}^\text{FD} \Delta_{\text{FLEX}}^\text{FD}$, leading to a non-monotonic behavior with $K_{ex}$. Figure 2 shows how changes in the number and duration of the mixing events influence the relative signal intensity of HetFLEX with respect to HMQC, both when considered on a per-scan as well as on a per-unit-acquisition-time basis. For the illustrated pH and temperature, $K_{ex}$ amounted to approximately 50 Hz, leading to $t_{\text{exch}} \approx 40$ ms as the optimum value (Figure 2a). As exemplified by the calculations in Figure S2, this is in agreement with what can be numerically estimated based on the proton transfer ratio $[PTR]$: Equation (1),\(^{[10]}\)

$$\text{PTR} = f_1 \lambda_{\text{HMQC}}^\text{FD} [1 - e^{-K_{ex} t_{\text{exch}}} - e^{-K_{ex} t_{\text{exch}}}]$$

where $f_1$ is the ratio between the solute and solvent pool concentrations, and $\lambda_{\text{HMQC}}^\text{FD}$ is the efficiency of the HMQC transfer. Using the latter as a fixed parameter, Figures 2b and c show how the HetFLEX signal intensity builds up as a function of the number of exchange loops $N$; note that

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**Figure 2.** Exploring the effects of different parameters in the Het-FLEX experiment. All data were acquired on a 100 mM $^{15}$N-labeled alanine sample in $D_2O/H_2O$ (2:8) at pH 2.2 and $T = 23.5$ °C. a) Calibration of the exchange time employed by the sequence in Figure 1a with 64 $t_1$ points, $t_2 = 0$, $N = 32$ exchange loops. b, c) Optimization of the number of loops using $t_{\text{exch}} = 40$ ms in the presence of varying concentrations of the relaxation agent GdDTPA affecting mostly the $T_1$ of the solvent. d) Relative intensities obtained using combinations of $t_{\text{exch}}$ and $N$ yielding the same total exchange time per scan.
comparing these plots with HMQC results (Figure 3, bottom),
overall similarities are evident, yet so are major differences.
On the one hand, the spectral resolution is worse in the 2D
HetFLEX spectra than in their conventional counterparts.
This is primarily due to the number of points in the HMQC
direct dimension being significantly higher than the one
achieved through HetFLEX, which is a consequence of the
increased acquisition dimensionality of the latter.
Furthermore, as the detection is attained through an exchange
process, the experiment is prone to yield broader spectra
despite the use of a constant $t_{\text{prep}}$ time. On the other hand,
although involving the same number of scans, the HetFLEX
peaks are approximately two orders of magnitude more
intense (in their integrated areas) than their HMQC counter-
parts. As for the $^{15}$N 1D spectra extracted from the 2D
HetFLEX version, these are identical to those of the 1D
version, apart from an approximately 18-fold increase in
intensity arising owing to the extra number of points ($16t_2$
increments) used to sample the new additional dimension.

In summary, the applicability of water-detected hetero-
nuclear NMR experiments based on CEST/FLEX proposi-
tions has been explored and demonstrated. The approach
enables the acquisition of 1D $^{15}$N and 2D $^{15}$N–$^1$H hetero-
nuclear correlation spectra for cases where the hydrogen
atom is in exchange with the aqueous solvent. Among the
drawbacks of this method is its relatively slow, indirect
detection nature, a feature that fast and ultrafast 2D
techniques could solve.[19] Its main advantage lies in the
substantial signal amplification that it delivers thanks to its
leverage of the abundant water resonance. While the
conditions conducive to this fast exchange were created for
small molecules by manipulating the pH value, these arose
spontaneously under physiological conditions for the studied
polypeptides. This opens HetFLEX perspectives for struc-
tural and dynamic assessments of disordered biomolecules.
A main technical obstacle that we confronted was the con-
comitant increase in noise associated with the detection of the
water resonance; we are currently exploring different options
to control this complicating artifact. Another dichotomy that
these approaches need to handle concerns the decreasing
efficiency of J-based transfers with increased solvent
exchange rates versus the increased efficiency of CEST/
FLEX with these increasing rates (Table 1). It is clear that in
many instances, more involved heteronuclear polarization
transfer approaches than HMQC should be adopted to deal
with this issue.[20] Other intriguing approaches concern the
adaptation of these protocols to include non-labile protons,
hyperpolarized systems, or non-aqueous solvents; these and
other extensions are currently under investigation.

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Conflict of interest

The authors declare no conflict of interest.

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R. S. Withers, J. Magn. Reson. 2006, 179, 290–293; b) K. Hashi,
S. Ohki, S. Matsumoto, G. Nishijima, A. Goto, K. Deguchi, K.

Figure 3. 2D $^{15}$N,$^1$H spectra obtained using HetFLEX (top) and HMQC (bottom) on the indicated samples, collected as indicated in Figure 1 a.


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Heteronuclear 1D and 2D NMR Resonances Detected by Chemical Exchange Saturation Transfer to Water

NMR resonances from heteronuclei can be detected through the modulation that they impose on a strong H₂O resonance (shown in red) by combining a 2D heteronuclear NMR sequence with a 2D NMR approach relying on chemical exchange saturation transfer principles (HetFLEX). 1D ¹⁵N and 2D ¹H/¹⁵N NMR spectra of small molecules and peptides can be recorded with substantial amplification.